

Integrated Mathematical Modelling for Cardio-Respiratory Dynamics: Diagnosis and Optimization of Treatment

¹Ms.S. Soundarya, ²Ms.R. Vidhya

¹Student, ²Assistant Professor

^{1,2}Department of Mathematics,

^{1,2}Bon Secours College for Women (Autonomous), Thanjavur-613006

Abstract : A highly integrated physiological network, the cardio-respiratory system is in charge of sustaining carbon dioxide elimination and oxygen supply, which guarantees appropriate cellular metabolism. Mathematical modelling has become a crucial tool for comprehending system dynamics and assisting therapeutic decision-making because of its intricate and nonlinear behaviour. This paper offers an integrated mathematical framework that uses differential equations to integrate oxygen transport, cardiac output, and pulmonary ventilation. Using control-theoretic techniques, the model integrates important physiological control systems including the Baroreflex and Chemoreflex. To examine system behaviour, numerical simulations are run under diseased, hypoxic, and normal settings. Additionally, optimising techniques are used to provide customised treatment plans, such as modifying oxygen therapy and optimising medication dose. The outcomes show how mathematical modelling may enhance biomedical system diagnosis, prognosis, and treatment.

IndexTerms - Cardio-Respiratory System, Mathematical Modeling, Differential Equations, Baroreflex, Chemoreflex, Oxygen Transport, Biomedical Engineering, Optimization

I. INTRODUCTION

1.1 Background of the Study

The cardio-respiratory system is essential for preserving physiological stability because it keeps tissues supplied with oxygen and eliminates waste products from metabolism, such carbon dioxide. This system allows for quick adaptability to changes like physical activity, environmental circumstances, and illness states by integrating the activities of the heart and lungs. Conventional clinical methods focus on observational data, which frequently misses the system's underlying nonlinear and time-dependent interactions. These dynamic processes may be systematically represented using mathematical modelling, especially with Ordinary Differential Equations. Researchers can forecast physiological reactions and get a better understanding of system behaviour by modelling factors like heart rate, breathing rate, and oxygen concentration.

1.2 Problem Statement

It is challenging to analyse the cardio-respiratory system using traditional techniques because it contains intricate connections between several physiological components. Among the main obstacles are:

- Time-varying and nonlinear system behaviour
- The respiratory and cardiovascular systems are strongly coupled.
- Why Traditional models' limited capacity to forecast the course of an illness
- The challenge of creating individualised treatment plans

It is difficult to correctly replicate physiological reactions under various situations, such as hypoxia or sickness, without a thorough mathematical foundation. An integrated model that can represent these relationships and aid in diagnostic and treatment planning is therefore required.

1.3 Objectives of the Study

The primary goals of this research are: • To create a comprehensive mathematical model of the respiratory and cardiovascular systems

- To use differential equations to depict physiological factors
- To include control systems like chemoreflex and baroreflex
- To model how a system might behave in both healthy and unhealthy circumstances.
- To use optimisation methods to enhance treatment plans

1.4 Scope of the Study

This research focuses on:

- Heart-lung interactions represented mathematically
- Utilising control theory and differential equations
- Modelling physiological states like illness and hypoxia
- Using optimisation methods while planning a course of therapy

The study lacks real-time clinical application and is restricted to theoretical modelling and simulation.

1.5 Motivation

Improving healthcare outcomes requires an understanding of the cardio-respiratory system's dynamic behaviour. Tools that can forecast how each patient will respond to therapy are needed to meet the growing demand for personalised care. The goal of this research is to close the gap between theoretical physiology and clinical practice by using mathematical approaches like differential equations and optimisation techniques. Such models can help physicians make better judgements and treat patients by offering predicted insights.

II. LITERATURE SURVEY

In biomedical research, mathematical modelling of physiological systems has been extensively studied, especially for comprehending the dynamics of the heart and lungs.

- In order to shed light on cardiovascular control systems, Mario Ursino (1998) created mathematical models that described the relationship between cardiac activity and baroregulatory processes.
- Michael C. K. Khoo (2000) developed thorough frameworks for physiological control system analysis, with a focus on estimate and simulation methods.
- John J. Batzel et al. (2007) emphasised the significance of coupled systems in physiological control by concentrating on modelling cardiovascular and respiratory dynamics.
- In 2009, James Keener and James Sneyd introduced sophisticated mathematical methods for physiological modelling, such as differential equations and nonlinear dynamics.

The intricate behaviour of biological systems may be accurately represented by mathematical models, according to earlier research. Integrated models that integrate several physiological subsystems and include optimisation strategies for clinical applications, however, are becoming more and more necessary. By putting forth a unified framework for cardio-respiratory modelling and therapy optimisation, this study expands on previous studies.

III. RESEARCH METHODOLOGY

A number of fundamental ideas underpin the mathematical description of cardio-respiratory dynamics:

ODEs, or ordinary differential equations:

Heart rate (HR), cardiac output (CO), respiratory rate (RR), and arterial oxygen concentration (PaO₂) are among the important physiological variables whose temporal evolution is represented by ODEs. The rate of change of each state variable as a function of interdependent physiological parameters is explicitly described by these equations.

linked Dynamical Systems: The mathematical models of the respiratory and cardiovascular systems must be linked due to their reciprocal interactions. For example, blood gas levels are determined by pulmonary breathing, and through chemoreceptor feedback loops, heart activity is modulated.

Control Theory: Physiological feedback mechanisms preserve homeostasis. Among these are the chemoreflex, which regulates blood gas (O₂/CO₂) levels, and the baroreflex, which modifies blood pressure. Negative-feedback differential equation frameworks are used to formally depict these control circuits.

Numerical Methods: Since the nonlinear, coupled differential equations that characterise cardio-respiratory physiology are usually unsolvable analytically, the dynamic behaviour of the system is simulated over time using numerical integration techniques like Euler's method and Runge Kutta methods, especially the fourth order (RK4) scheme.

Optimisation Techniques: To identify the best treatment interventions, such as medication dose or ventilator oxygen-flow settings, mathematical optimisation is used. Techniques that are applicable include: Gradient-based optimisation The use of genetic algorithms Sensitivity study of parameters The integrated cardio-respiratory model is based on these computational and mathematical techniques.

IV. RESULTS AND DISCUSSION

Cardiac Model:

Heart rate (HR) and stroke volume (SV) determine cardiac output (CO). The following provides a simple dynamical representation:

where a_2 is the decay constant and a_1 is the stimulation constant.

$$\frac{dCO}{dt} = a_1(HR \cdot SV) - a_2CO$$

Respiratory Model:

As a function of tidal volume (TV) and respiratory rate (RR), pulmonary ventilation (\dot{V}) is represented as a dynamic variable. The following first-order equation can be used to represent its rate of change.

$$\frac{d\dot{V}}{dt} = k_1 \cdot RR \cdot TV - k_2 \cdot \dot{V}$$

Oxygen Transport Model:

A mass balance between pulmonary absorption and peripheral tissue consumption via tissues controls the arterial oxygen content ([O₂]_a):

$$\frac{d[O_2]_a}{dt} = \alpha \cdot \dot{V} \cdot (P_{IO_2} - P_{AO_2}) - \beta \cdot M$$

where:

- α is the lung gas-exchange efficiency
- β is the metabolic coefficient
- M represents the tissue metabolic rate
- P_{IO_2} and P_{AO_2} are the inspired and alveolar oxygen partial pressures, respectively

Coupling of Subsystems:

This formulation illustrates the fundamental feedback structure of the cardio-respiratory system by capturing the integrated dynamics between ventilation, perfusion, and oxygen availability.

Baroreflex and Chemoreflex Reflex Controls:

In reaction to a drop in arterial oxygen tension (hypoxia), the chemoreflex system increases both heart rate and breathing rate. A control function, like this one, models this physiological reaction:

$$HR_{chem} = HR_0 + G_c \cdot \max(0, P_{aO_2,ref} - P_{aO_2})$$

where PaO₂ is the partial pressure of arterial oxygen, G_c is the chemoreflex gain, and HR₀ is the baseline heart rate.

The baroreflex regulates cardiac contractility, vascular tone, and heart rate to stabilize blood pressure. Its regulating function is recognized as an essential part of cardiovascular homeostasis, even if its whole dynamics are not clearly depicted in this reduced framework.

Simulation and Analysis:

A numerical integration methodology, namely the fourth-order Runge–Kutta (RK4) method, was used to simulate the integrated model over a 60-second period. Standard adult resting-state values were used to determine the initial conditions:

- Cardiac Output (CO) = 5 L/min
- Heart Rate (HR) = 75 beats per minute (bpm)
- Respiratory Rate (RR) = 12 breaths per minute
- Arterial Oxygen Saturation (SpO₂) = 95%

Normal Physiology:

The model displays steady homeostatic behaviour under simulated resting conditions:

- Heart rate stabilizes between 70–80 bpm.
- Respiratory rate stabilizes between 12–14 breaths per minute.
- Arterial oxygen saturation is maintained near 98% via physiological feedback.

Hypoxia Simulation:

When arterial saturation drops below 93% in response to a simulated hypoxic event (such as inspired oxygen decrease), the following compensatory reactions are seen:

- Heart rate increases due to chemoreflex activation.
- Respiratory rate elevates to enhance alveolar ventilation.
- Consequently, arterial oxygen saturation recovers toward its physiological set-point (~98%).

The body's acute homeostatic correction for hypoxia is accurately replicated by this mimicked reaction.

Pathological Conditions:

Modified dynamic responses under different illness states may be simulated by the model.

Decreased Ventilation Efficiency in Chronic Obstructive Pulmonary Disease (COPD)

There is a delayed and muted ventilatory response.

Recovery of oxygen is sluggish and frequently insufficient.

The cardiovascular system is chronically stressed by a consistently high heart rate.

Heart Failure

Chronic tissue hypoxia is brought on by decreased cardiac output.

To completely restore oxygenation, compensatory increases in respiratory rates are inadequate.

These examples show situations when therapeutic intervention—like optimal medication dosage—is necessary.

These simulations show how useful the model is for examining the pathophysiology of diseases and evaluating the effectiveness of possible treatment approaches.

Diagnosis And Treatment Optimization:

Personalised medicine is based on the ability of physicians to forecast how each patient will react to therapeutic interventions using mathematical models.

Sensitivity Analysis:

The physiological elements that have the most impact on systemic oxygen levels are found using a parameter sensitivity study. Important influencing factors consist of: Efficiency of ventilation

- The reactivity of heart rate
- Decay rate of cardiac output

In order to measure clinical dysfunction, these sensitive characteristics may be used as diagnostic indicators.

Sample problem

Problem Statement: Take a look at a basic cardio-respiratory model that explains how blood oxygen saturation and heart rate interact:

$$\frac{dO_2}{dt} = 0.1(V - CO) - 0.05 O_2$$

$$\frac{dHR}{dt} = 0.2(98 - O_2) - 0.1 HR$$

where:

- $O_2(t)$ = arterial oxygen saturation (%)
- $HR(t)$ = heart rate (beats/min)
- Constant Ventilation rate $V=6$ L/min
- Constant Cardiac output $CO=5$ L/min.

Initial conditions:

$$O_2(0) = 95\% , \quad HR(0) = 75 \text{ bpm}$$

Questions:

1. Determine the oxygen level at equilibrium.
2. When oxygen falls below equilibrium, analyse the heart rate response.
3. Determine the initial heart rate change rate.
4. Describe the model's physiological significance.

Solution:

1. Equilibrium Oxygen Level:

At equilibrium:

$$\frac{dO_2}{dt} = 0 \quad \text{and} \quad \frac{dHR}{dt} = 0.$$

From the oxygen equation

$$0 = 0.1(V - CO) - 0.05 O_2^{eq}$$

Substituting the given values $V = 6$ and $CO = 5$:

$$0 = 0.1(6 - 5) - 0.05 O_2^{eq}$$

$$0 = 0.1 - 0.05 O_2^{eq}$$

$$O_2^{eq} = \frac{0.1}{0.05} = 2$$

Equilibrium oxygen level: $O^{eq} = 2\%$

Heart Rate Response to Hypoxia:

$$\frac{dHR}{dt} = 0.4(98 - O_2)$$

Heart rate equation:

- If $O_2 < 98$, then $98 - O_2 > 0$
- Hence $\frac{dHR}{dt} > 0$

Initial Rate of Change of Heart Rate

At $t = 0$, $O_2 = 95$: and $HR(0) = 75$. Substituting into the HR equation:

$$\begin{aligned} \left. \frac{dHR}{dt} \right|_{t=0} &= 0.2(98 - 95) - 0.1 \times 75 \\ &= 0.2(3) - 7.5 \\ &= 0.6 - 7.5 = -6.9 \end{aligned}$$

Initial change in heart rate:

-6.9 beats per minute. This negative number shows that the heart rate is initially declining toward equilibrium under the specified beginning conditions.

Physiological Interpretation: The mechanism stabilises oxygen levels by displaying negative feedback.

Oxygen Equation: Controlled by mass balance, oxygen saturation decreases proportionately to its present level due to tissue consumption and increases with the net surplus of ventilation over cardiac output (oxygen intake minus circulatory removal).

Heart Rate Equation: This serves as a controller for proportional feedback. In relation to the 98% physiological set-point, the phrase (98-O₂) produces an error signal that causes heart rate corrections.

Integrated System: These formulas work together to provide the negative feedback loop that is necessary for homeostasis: as oxygen levels fall, heart rate rises, increasing cardiac output and oxygen delivery and bringing oxygen levels back to the set-point.

Final Answer

Question	Answer
Equilibrium oxygen level	2%
HR response to low O ₂ level	HR increases via chemoreflex activation
Initial HR change	-6.9 bpm/ min
Model meaning	A negative-feedback control system modelling cardio-respiratory homeostasis

REFERENCES

- [1] Mario Ursino, "Carotid baroregulation and the pulsating heart: A mathematical model," American Journal of Physiology-Heart and Circulatory Physiology, 1998.
- [2] Physiological Control Systems: Analysis, Simulation, and Estimation by Michael C. K. Khoo. Wiley-IEEE Press, Piscataway, NJ, USA, 2000.
- [3] "Modelling cardiovascular and respiratory dynamics," John J. Batzel et al., Annals of Biomedical Engineering, 2007.
- [4] Mathematical Physiology, James Keener and James Sneyd. Springer, New York, NY, USA, 2009.

Copyright & License:

© Authors retain the copyright of this article. This work is published under the Creative Commons Attribution 4.0 International License (CC BY 4.0), permitting unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.